A Review of The Properties of The Pulmonary Artery in Pulmonary Arterial Hypertension with Emphasis on The Water Hammer

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Introduction

Definition of Pulmonary Hypertension

Pulmonary hypertension is defined as resting average pressure, measured with a right heart catheter, in the pulmonary artery ≥ 25 mmHg [1]. According to the current data situation, normal average pressure in the pulmonary artery has a maximum value of 20 mmHg [2]. Patients with values between 21 and 24 mmHg (= Borderline pulmonary hypertension) should, according to the most recent guidelines of the [3] European Society of Cardiology (ESC), not be treated. Regular check-ups are, however, necessary. The diagnosis of pulmonary hypertension can only be made using resting measurements, earlier definitions such as “load-induced pulmonary hypertension” are no longer valid, according to the newest studies [4]. Depending on Pulmonary Capillary Wedge Pressure (PC) and Pulmonary Vascular Resistance (PVR), different hemodynamic definitions of pulmonary hypertension exist, with corresponding clinical symptoms [5].

Pulmonary Artery Compliance (CPA)

The transfer of pressure through the entire circulation and control of blood flow are necessary preconditions for the development of pulmonary circulation. For these tasks to be fulfilled optimally and taking into account the normally low pressure in the pulmonary circulation, the pulmonary arteries must normally show high elasticity (compliance) [6]. The relationship between pressure and volume, called volume elasticity or arterial compliance, is used to describe this issue. This is usually defined by the quotient:

\[
\text{Compliance(C)} = \frac{\text{(stroke volume)}}{\text{(pulse pressure)}} = \frac{\text{SV}}{\text{PP}}
\]

where: pulse pressure = systolic pressure minus diastolic pressure.

This calculates the blood volume that can be accommodated in a vessel, with a predefined diameter, at a known pressure. An
artery with high compliance, is called an elastic artery, one with low compliance, is a stiff artery [7,8]. The importance of compliance lies in the fact that an artery with high compliance can store a relatively large quantity of the blood expelled from the ventricle during the systole and then release this volume in the diastole, so that there is a continuous flow into the pulmonary circulation [9]. Arteries with low compliance do not have this ability and their contribution to the diastolic flow is small [6,7]. Compliance was already an essential element of the two-element model [10] in the first description of the arterial air-vessel (windkessel) in the year 1899 and was also used in the three [11] and four-element windkessel model [10]. These descriptions tried to explain how the arterial system worked. The air-vessel model of the pulmonary circulation is based on the function of a fire brigade air-vessel (Figures 1 & 2). The pump (heart) conveys the water (blood) to the air vessel (elastic artery). The compressed air in the air vessel was a storage function (compliance) which makes it possible to distribute the water faster and with higher pressure.

The change in compliance in PAH is a more decisive factor in the development of the prognosis and the treatment of the patients. There are clinical [11,12] and experimental [13] indications that the reduction in compliance is a decisive parameter in the multifactorial genesis of the disease. The reduction occurs simultaneously with the increase in PVR [7]. Therefore, in contrast to the other vascular property’s compliance is always reduced in patients with PAH, irrespective of the etiology of the PAH [14]. In order to understand the independent role of compliance better, Sajanet (15) examined its relationship to the clinical evaluation and the symptoms of PAH. They discovered that a reduction in compliance accompanies the increase of various hemodynamic parameters (PAm, PVR, RA-pressure) and a worsening of resilience (shorter distance walked in the 6-minute walk test) as well as being associated with an increased likelihood of an inpatient stay [15]. An increase in compliance can be achieved as a sign of a hemodynamic improvement. Specialized drug therapy with bosentan and sildenafil leads to an improvement in the SV/PP ratio in PAH patients, together with an increase in resilience [16].

**Pulmonary Vascular Resistance (PVR)**

Vascular resistance is a quantitative description of the relationship between the pressure difference along the vessel and the blood flow [6]. Although the resistance can be calculated with Poiseuille’s law, Ohm’s law is used in daily clinical practice [17]:

\[ R = \frac{\Delta P}{Q} \]  

(II)

Where: \( R \) = resistance, \( \Delta P \) = pressure difference, \( Q \) = blood flow.

The result of applying this law for the pulmonary circulation, is the equation for pulmonary vascular resistance:

\[ \text{PVR} = \frac{\text{PAm-PC}}{\text{CO}} \]  

(III)

Where: PVR = Pulmonary Vascular Resistance, PAM = Average Pulmonary Artery Pressure, PC = Pulmonary Capillary Wedge Pressure, CO= Cardiac Output.

Resistance is a component of the two-element windkessel model [17] and also remains in the three [11] and four element windkessel models [10]. Together with compliance and impedance, it is one of the three elements on which the RV afterload depends [17]. The pulmonary circulation resistance is significantly lower in comparison with the systemic resistance. It increases in PAH [1,3,4]. The clinical importance of this parameter has been known for a long time. A value above six WE in patients with terminal heart failure and before heart transplantation, is linked to an increased probability of acute right heart failure postoperatively (up to 28 % in the first three months [18]). For this reason, according to the international Medical Association guidelines, PVR > 6 WE is an exclusion criterion for a heart transplant but not for a combined heart-lung transplant [19]. The value, particularly in the diagnosis and treatment of PAH, is unarguable. Not only is a PVR above three Wood units, a part of the definition [2], but this cut-off value can also be used to distinguish between isolated post-capillary and mixed post- and pre-capillary, pulmonary hypertension [3]. Therefore, according to the most current European guidelines [3], the measurement of PVR is necessary for every right heart catheter examination. In addition, there are signs that, after a point in the natural course of PAH, the rise in PVR becomes steeper [2-24]. A decrease in PVR is considered an indicator of a patient’s hemodynamic improvement [7,9,14], although there is no clear linear correlation with the clinical picture [14,18].
Water Hammer Phenomenon

A known phenomenon that occurs in every pump system with rapid change in flow (due to valve opening and closing) is the Water Hammer [25,26]. Water Hammer is a wave of pressure, which due to a rapid change in flow and the resulting changes happen due to start/stop of the pump and opening or closing of a valve. The acute change of state of the pump and/or valve result in a change in momentum (defined as the product of mass X velocity) of the fluid. This change in momentum produces a shockwave, which under certain circumstances causes damage in the pipes of the pump system. The damage occurs when the applied force of the shockwaves overwhelms the elastic capacity of the pipes. The effects of such a phenomenon are not independent of the geometry of the pipe system. For example, when a water hammer wave reaches a bifurcation or an increase in cross-sectional area, there is a reduction in the amplitude of the wave. With increased resistance (or afterload in terms of hemodynamics) there can be an increase in the amplitude of the reflected wave of the water hammer, especially in systems with a closed end. In general, under certain conditions (or afterload in terms of hemodynamics) there can be a reduction in the amplitude of the wave. With increased resistance (or afterload in terms of hemodynamics) there can be an increase in the amplitude of the reflected wave of the water hammer, especially in systems with a closed end. In general, under certain conditions =water hammer pressure are multiplied [27].

The mathematical equations describing this phenomenon are [25,26]:

\[ \frac{\partial u}{\partial x} + \frac{1}{B} \frac{\partial u}{\partial x} = 0 \]  \hspace{1cm} (IV)

and

\[ \frac{\partial u}{\partial t} + \frac{1}{\rho} \frac{\partial u}{\partial x} + \frac{f}{D} \left| \frac{\partial u}{\partial x} \right| = 0 \]  \hspace{1cm} (V)

\[ u = \text{velocity}, \ P = \text{pressure}, \ t = \text{time}, \ X = \text{space}, \ f = \text{factor of viscosity}, \ B = \text{module of elasticity,} \ \rho = \text{density}. \]

and the modified equation is

\[ \frac{\partial p}{\partial t} = \rho \text{PWV} \frac{\partial V}{\partial x} \]  \hspace{1cm} (VI)

with PWV being pulse wave velocity.

This phenomenon is nothing more than a manifestation of energy transformation from kinetic to dynamic energy due to the different compression ability between the fluid and the pipes of the pump system. The enhanced pressure is transformed in extra compression of the pipe and therefore, a higher initial velocity will produce a more intense compression of the pipe wall. The water hammer phenomenon describes this dynamic change in a closed pipe system, when an acceleration or deceleration of the flow occurs. It plays a more significant role in pipe systems with low pressure, such as the pulmonary circulation [21,22].

What Correlations are there Regarding the Pulmonary Circulation?

The importance of PWV in the evaluation of arterial properties has been demonstrated by several studies: [23] PWV is the most validated method for noninvasively quantifying arterial stiffness. It is regarded as the gold standard due to its simplicity, reproducibility, and clinical relevance [24]. The definition is basically rational: the systolic period produces a pulse that leaves the ventricle and enters the vascular system. Its velocity is the distance between two points of the cycle divided by time [21]. Increased arterial stiffness leads to increased speed of the pulse wave in the artery [22]. PWV is calculated with the Moens-Korteweg form:

\[ \text{PWV} = \sqrt{\frac{Eh}{2\rho}} \]  \hspace{1cm} (VII).

Eh is Young’s modulus for elasticity (the ratio stress / strain), r is the radius of the vessel (measured in mm), h is the wall thickness (measured in mm) and \( \rho \) the blood density. A relationship between PWV and compliance (inversely proportional) has also been demonstrated [28-30]. This means that a stiffer artery leads the pulse wave much faster compared to an elastic artery. The significance of arterial stiffness is undoubtedly proven. It is an independent risk factor for the development of coronary heart disease (HR 1.23, 95% CI 1.11 to 1.35), an ischemic stroke (HR 1.28; 95% CI 1.16 to 1.42) and peripheral arterial disease (HR 1.30, 95% CI 1.18 to 1.43) and has statistical significant correlation with cardiovascular (HR 1.28 95% CI 1.15 to 1.43) and total mortality (HR 1.17, 95% CI 1.11 to 1.22) [27]. Kaess et al. [28] further investigated the correlation between stiffness and blood pressure and found that although the presence of stiffness is associated with an increased probability of developing hypertension, the development of arterial stiffness remains independent [28].

According to (VII) PWV and the rate of change of pressure of the artery (dp/dt) are proportional. Two processes are responsible for this:

a) The elastin and collagen deposits in the extracellular matrix, which shift the power deformation curve (F(\lambda) curve) to the left [29],

b) And the (particularly in PAH) increased right ventricular stress, which is transmitted into the PA [30].

The presence of the water hammer phenomenon in the arterial system and the human body has been previously mentioned and used. Vennin et al. [31] have accomplished to deliver the aortic pressure from the aortic flow using the above equations and Harald et al.[32] have confirmed the measurements in vivo. The mathematical dependency of PWV and dp/dt has also been experimentally proven [33-35]. At this point it should be further analyzed which role has the arterial stiffness in the pulmonary circulation. Elasticity is the property that permits the transformation of the wall due to an applied force and by withdrawing of this force the wall returns to its initial shape. This is not the case in the human cardiovascular system, as the arterial walls are not elastic but viscoelastic. This means that a rapid application of force has more loss of energy than a slow one [6]. This is because, a larger rate of change of pressure means greater applied force, which results a greater velocity of stretch and therefore greater viscosity. This increase in viscosity...
means, that a greater energy loss is taking place during the systolic period and that the ventricle must produce a greater energy in order to retain the same stroke volume. Due to the viscoelastic nature of the human arteries, the increased stiffness of the pulmonary artery in patients with pulmonary hypertension the presence of the water hammer cannot be excluded.

What is the Meaning of the Water Hammer in Pulmonary Hypertension?

The current treatment of PAH can be divided into three levels: General measures, supportive therapy and targeted/specific PAH treatment. General measures should be understood as the avoidance of pregnancy, routine influenza and pneumococcal vaccination, avoiding travel in altitudes over 1500 to 2000 m, psychosomatic, psychological and social patient counselling. The supportive measures include the administration of diuretics for signs of right cardiac decompensation, oxygen therapy at pO$_2$ < 60 mmHg and iron replacement in cases of iron deficiency anaemia. Targeted PAH treatment, consisting of endothelin receptor antagonists, phosphodiesterase-type-5 inhibitors, guanylate cyclase stimulators and the prostanoids aim to vasodilatation, increase of the vessel elasticity, reduction of the vascular resistance and improvement of the right ventricular function [36,37]. In engineering however, the treatment of the water hammer cannot be the increase of the pipe elasticity, since the elastic properties of pipes in a given system can no longer be changed and the following methods are used: - The installation of a by-pass pipe with a non-return valve. It does not prevent the water hammer effect, but it can reduce the magnitude of the water hammer wave.

A reduction approximately of 33% can be achieved [38]. Another alternative is the surge tanks in piping system. These tanks act as a reservoir to suppress the pressure waves and are installed on the discharge pipe. When the pressure in the pipe increases, a dense fluid enters the tank and is stored locally. During periods of subnormal pressure in the pipe, the fluid would flow back to the pipe, preventing rapid velocity changes [38]. Finally, the installation of air chambers. Air chambers are basically a type of high-pressure surge tanks which can be built in small sizes. In these tanks, the pressurized air locates on the top of liquid separately. The size of the chamber must be large enough to compensate the liquid in the subnormal pressure periods [38]. Among water hammer damping devices, air chambers are often used to reduce pressure surges of system to acceptable values. The chamber is more effective if a throttling device is used, resulting in a reduction of the required volume [39]. Although the application of such methods in the human body seems difficult and problematic, a proper use could be an alternative in patients where the medical treatment is no longer sufficient and a transplantation is not a suitable option. Experimental and clinical studies are obviously necessary in order to move in a such direction.

Conclusion

Water hammer seems to be also manifest in the pulmonary artery of patients with pulmonary arterial hypertension and is already being used in computation of various problems. A deeper understanding may result in newer solutions regarding the treatment of diseases.

References


